Fixed Field Alternating Gradient for Muti-turn Superconducting ERL and Medical Applications

An introduction the Fixed Field Alternating (FFA) Gradient accelerators will be provided with pros and cons for accelerating particle beams. A design, installation, and commissioning of the 'CBETA' (**C**ornell University Brookhaven National Laboratory ERL Test Accelerator) is shown. A new and an existing FFA approach for the FLASH proton cancer therapy accelerator and the proton delivery gantry with permanent magnets will be presented. A single beam line ERL LHeC lattice for the future Electron Ion Collider at LHC is shown.

Fixed Field Alternating Gradient for Muti-turn Superconducting ERL and Medical Applications

- 1. Brief history of accelerators
- 2. Fixed Field Alternating (FFA) Gradient Accelerators
- 3. Non-Scaling FFA gradient accelerators
- 4. New FFA Superconducting Multiturn ERL CBETA
- 5. FFA lattice for LHeC
- 6. Permanent and Superconducting Magnet FFA proton and carbon Gantry
- 7. Fast Cycling FFA proton Synchrotron

BRIEF HISTORY OF ACCELERATORS

Leó Szilárd, Rolf Widerøe, Gustav Ising designed the first linear accelerator (1924)

Ernest Lawrence - 1930 cyclotron built at Berkeley – Nobel Prize in Physics

Kolomensky, Ohkawa, Symon and Kerst Fixed Field Alternating Gradient (~1950)

E. D. Courant, M. S. Livingston and H. S. Snyder, The strong-focusing alternating synchrotron (1952) at BNL

Linear Accelerator

A linear particle accelerator (linac): Increases the velocity of ions by subjecting them into a series of oscillating electric fields potentials along the beam line.

(invented by Leó Szilárd, patented by Rolf Widerøe 1928, idea fist published by Gustav Ising).





STRONG AND WEAK TRANSVERSE FOCUSING

To build a relativistic cyclotron, the field needs to grow proportional to γ , giving vertical defocusing, and compensate with focusing edges. This is an early form of "strong focusing".

If the focusing was still insufficient the reverse bends are added. That's how the Fixed-Field Alternating Gradient machine FFAG was invented.











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The KEK and KYOTO University 150 MeV Scaling FFA Gradient proton Accelerator



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Dispersion Function vs. Momentum



Normalized Dispersion Space



The amplitude value of '*H*' is determined within the bending element. It is enough to minimize '*H*' within the dipole to obtain the minimum. The average value of the '*H*' function is always proportional to the : $(\rho\theta)^3$ and a merit factor *F* in minimization had been previously introduced as:

$$< H > \approx F \rho \theta^{3}$$
 $\frac{d}{dD_{o}} < H > = 0, \quad \frac{d}{dD_{o}} < H > = 0, \quad \frac{d}{d\beta_{o}} < H > = 0$

To minimized the dispersion function **7** the BENDING MAGNET (DEFOCUSING) should be in the middle with

minimum of D_{xmin} and β_{xmin} at the center



SCALING VS. NON-SCALING FFAG



Linear magnetic field: $B = B_o + r G_o$



- Orbit offsets are proportional to the dispersion function: $\Delta x = D_x * \frac{\delta p}{p}$
- To reduce the **orbit offsets to \pm 4 cm range**, for momentum range of $\delta p/p \sim \pm 50$ % the dispersion function D_x has to be of the order of:

 $D_x \sim 4 \ cm / 0.5 = 8 \ cm$

Non-scaling FFAG for Muon Acceleration

 $\Theta_{0F} = -0.027$ Total Circumference C = 328 m $L_{of} = 0.58 \text{ m}$ Cell length = 4.9697 mN=66 Number of cells N = 66- Extremely strong CELL LENGTH 5 m = 33.3% focusing with a small QD QF 47.8 mm QF dispersion function $r \delta p/p = 0$ - Tunes vary Drift for a cavity -29.5 mm $0.5 L_{cav} = 0.992 m$ - Orbit offsets are small = -33.3% - Magnets are small $L_{m} = 0.163 \text{ m}$ - Large energy acceptance s=0 $s = 0.5 L_{\text{CELL}}$ $L_{00} = 1.5 \text{ m}$ $\Theta_{\rm OD} = 0.1436$ PHYSICAL REVIEW SPECIAL TOPICS - ACCELERATORS AND BEAMS 8, 050101 (2005)

Design of a nonscaling fixed field alternating gradient accelerator

D. Trbojevic,^{*} E. D. Courant, and M. Blaskiewicz BNL, Upton, New York 11973, USA

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Cornell University Brookhaven National Laboratory Electron Test Accelerator - CBETA



- 1. Full proof of principle for the Non-scaling Fixed Field Alternating Gradient
- 2. Merging multiple energy orbits into a single straight-line orbit
- 3. Development of the new permanent magnet technology









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What is 'CBETA'

- Cornell DC gun, 2nC peak
- 100mA, 6MeV SRF injector (ICM), 1.3GHz
- 320mA, 6-cavity SRF CW Linac (MLC), 1.3GHz
- 4 Spreaders / Combiners with electromagnets ٠
- FFA cells with permanent magnets, 3.8 energy aperture, 7 beams



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CBETA Preparation Spring 2015

70% of the existing technical-use space was removed for the initial phase



CBETA Spring 2019



Novelties in CBETA

•ENERGY RECOVERY MULTITURN LINAC WITH WITH 4 TURNS DURING ACCELERATION AND FOUR TURNS DURING THE ENERGY RECOVERY

•SUPERCONDUCTING RF : INJECTOR AND MAIN LINAC CRYOMODULE

•NON-SCALING FFAG – MULTI ENERGY SINGLE BEAM LINE

- FFAG ARCS
- TRANSITION FROM ARC-TO-STRAIGHT
- STRAIGHT SECTION WITH MULTI-ENERGY TRANSFER

•PERMANENT HALBACH TYPE COMBINED FUNCTION MAGNETS

Established new permanent magnet technology



Permanent Combined Function Magnet Design



Halbach design made of NdFeB material

This is a combined dipole+quad

Being measured on rotating coil at BNL

3D printed multipole corrector pack inside

Windo wframe corrector coil outside

Temperature stabilised by water (orange hoses)

Fixed-Field Return Arc





Merging of Multiple Energy Orbits in the arcs to the Straight Section into a Single Orbit



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Commissioning results: orbit correction in fixed-field loop





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Two Turns with Orbits Uncorrected

(October 23, 2019)



Measured Two Turns with Corrected Orbit



(November 8, 2019)



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Tunes in FFA part Compared to Model





7-turn ERL operation with corrected turns 1,2,3



Achieved Parameters

Cornell DC gun

- 75mA short term, 65mA for hours
- Detailed **phase space diagnostics** for space charge dominated beams.
- Study of 2nC bunch charges
- High power SRF injector linac
- Tested up to 13.5MeV
- Tested up to 75mA
- Investigation of ion / beam interactions

ERL main SRF linac

- Operated with 1-turn ERL and 99.4% ERL efficiency
- Operated with 4-turn ERL
- Detection of micro bunching
- 1-turn current limited to 70mu for radiation protection.
- 4-turn current limited to 1nA because of 50% beam loss in the last recovery loop. FFA return loop
- 7 simultaneous beams (at 42, 78, 114, 150MeV)
- Hardly measurable beam losses in the FFA region

DC gun results



Beam to the Linac lost at the splitters

First beam Dec. 24, 2019. Multi-turn energy recovery achieved on operated until February 2020.



Beam in the beam stop line



Before the 7th FFA pass there remains an unresolved 60% loss

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Energy Recovery in every Cavity

- Transmission 99.6 \pm 0.1%; energy recovery > 99.8%
- Measured up to 8 μ A
- Each cavity accelerates beam without receiving external power for it.



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SUMMARY

- First multi-turn SRF ERL
- Full Proof of Principle for the Non-Scaling Fixed Field Alternating Gradient Concept
- Proof of Principle for the ARC to Straight Merging
- Established New Technology for the superb quality Halbach-type permanent Combined Function
- Opened door for application to the new electron-positron and electron ion colliders with permanent magnets
- Established energy saving measures: Energy Recovery, SRF, and permanent magnets.

Application of the FFA concept to the possible future energy upgrade of RLA at Jefferson Laboratory from 12 to 22 GeV and alternate FFA DESIGN FOR LHeC

Layout of the LHeC-LHC-SPS

From Oliver Brüning, Andrei Seryi, and Silvia Verdu-Andres Frontiers in Physics, 25 April 2022, Electron-Hadron Colliders: EIC, LHeC and FCC-e



FIGURE 2 (A) Layout options and footprint of the LHeC in the Geneva basin next to the Geneva airport and CERN. The yellow racetrack corresponds to the LHeC layout that offers optimal performance; in orange, two size variations explored for cost optimization. For reference, the light blue circle depicts the existing tunnel of the LHC; the dark blue circle is the SPS. (B) 3D schematic showing the underground tunnel arrangement. The grey sections indicate the existing SPS and LHC tunnel infrastructures and the yellow section the new LHeC installation.

FFA LHeC Recirculator with Energy Recovery



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Lattice Functions in a Cell for the WEST-FFA arc

Magnet Properties:

Focusing Magnet QF GF= -73.26375 T/m QLF= 1.5 m θ_F =-0.023180154 B_F=1.07218 T B_{FMAX}=-1.25 T

Defocusing Magnet BD GD= -73.26375 T/m BLD= 0.7511 m θ_D =-0.023180154 B_D= -0.71375 T B_DMAX=-1.755 T

Total Synchrotron Radiation Lost In the West Arc from five passes:

E_{LOSS}=373.7 MeV



Lattice Functions in a Cell for the EAST-FFA arc

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Applications of the FFA concept to the Cancer Radiation Therapy Accelerators, Beam Lines and Gantries

FLASH therapy in the existing proton therapy systems



FFA Beam lines with 70–250 MeV kinetic energy range



Present VARIAN-SIEMENS gantry



Permanent Magnet Gantry



Fast Cycling FFA Synchrotron

The proposal is based on the existing US patent by the PI of this proposal: D. Trbojevic, Title: "Non-scaling fixed field alternating gradient permanent magnet cancer therapy accelerator", patent number: US 9661737 B2, Date of the patent: May 23, 2017 (belongs to the DOE).

https://patentimages.storage.googleapis.com/42/5e/92/f7da1cf617d6e3/US9661737.pdf



Matching of the Multiple Energy Orbits to the Straight Section



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14

14

Injection, Extraction and three RF cavities



Synchrotron Beam Size Estimates from the 10 MeV cyclotron

- Input beam is assumed to come from
- the 10 MeV cyclotron
- Measured emittance ~5 π mm mrad
 - $\sigma_{n} = \sqrt{\frac{\beta_{twiss}\varepsilon_{n}}{6\pi \gamma\beta}}, \quad 95\% \quad = \quad \sigma_{x} = 1.517 \text{ mm}$ $\varepsilon_{n} = \frac{6\pi \gamma\beta \sigma_{n}^{2}}{\beta_{twiss}} \quad \sigma_{y} = 2.398 \text{ mm}$ At Injection kinetic energy is 10 MeV $\gamma = 1.010657 \ \gamma \beta = 0.14484$ $\gamma\beta = \sqrt{\gamma^2 - 1} / \gamma$ G_{F18}=155 T/m B_{F18}= -0.281 T RMS [mm] Profile Meas. 5.238 MA25X **OPAL 2.386** 0.8 10.6 cm 7.6 cm L4 mm Ē Wound 0.4 0.2 -40 -30 -20 10 20 30 40 -10 0 Good Field Region Position [mm] 18.6 mm Good Field Region 13.3 mm Ref. [28] 9.1 cm

Figure 8: Two oval combined function defocusing (left) and focusing magnet (right) designs of the highest magnetic fields, with beam sizes at both proton kinetic energies of 70 (right side) and 250 MeV (left sides) with the 'PROSCAN' measured beam profile (right) after the degrader and collimators.

8 cm

β_x~ 0.4 m

 $\beta_v \sim 1 \text{ m}$

Tunes vs Energy in the FFA Synchrotron



Time of flight dependence during acceleration



Orbits in the FFA synchrotron After Dynamical Aperture Improvements



Dynamical Aperture Studies

Transverse Field in the Magnet Dependence on Radial Offset Fiixed Betatron Tunes FFA synchrotron 66 Cells in the full Circle nux=0.246, nuy=0.0814 09-22-2022



Permanent Magnets with additional Multipoles



Magnetic field dependence on Energy





Proton Kinetic Energy (GeV)

Application of Fast-Cycling FFA Synchrotron for Proton Cancer FLASH Radiation Therapy

FLASH cancer therapy: Multiple biological studies and even few patients' treatments around the world in recent years confirmed significant improvements in the cancer treatment results; termed FLASH radiotherapy, involves delivering the same treatment dose *but in much shorter time intervals* — fractions of a second as opposed to minutes — and in far fewer fractions or even a single fraction and therefore at dose rates that are thousands of times higher [1].

The 10 MeV commercially available cyclotron has frequency of 42 MHz and provides 120 mA. This makes 1.8×10^7 protons per bunch. As the synchrotron accelerates 30 bunches this makes per each synchrotron cycle $N_{PROTONS} = 1.15 \times 10^8 \times 30 = 5.4 \times 10^7$. To achieve the 3.8 x 10^{11} protons for FLASH therapy it is required to run the synchrotron per one FLASH treatment N=3.8 x $10^{11}/3.23 \times 10^{9}$ ~ 700. The total time for the FLASH treatment is $t_{FLASH}=700 \times 898 \ \mu s = 632 \ ms!$

[1] Konrad P. Nesteruk and Serena Psoroulas, "FLASH Irradiation with Proton Beams: Beam Characteristics and Their Implications for Beam Diagnostics", applied sciences, 2021, 11, 2170, https://doi.org/10.3390/app11052170

SUMMARY

- The 10-250 MeV fast cycling proton synchrotron with cycling of 1.3 kHz is the fastest synchrotron proposed. The synchrotron rates are in a range are 15-60 Hz.
- In proton acceleration within the non-relativistic energy range the main problem is the limitation on the speed of magnetic field response to the change of energy. This limitation is now eliminated by using the permanent magnets for the same energy range.
- One of possible application is in FLASH cancer radiation therapy.
- This proof of principle accelerator would enable new areas of research using the same principle but building the magnets with multi-layer superconducting wires.

Advantages:

- 1. The Fast-cycling permanent magnet synchrotron with 6x10 m area is the best possible synchrotron for the cancer proton FLASH radiation therapy it is cost efficient, does not require electrical power, magnets are very small and light.
- 2. Small, energy efficient, and fast cycling proton drivers for NPP and HEP.
- 3. Future Fast cycling synchrotron accelerator driven system (ADS) for transmutation of nuclear waste.